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Gadolinium nanoparticles and contrast agent as radiation sensitizers

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Running title: GdNPs as radiation sensitizers

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ABSTRACT

The goal of the present study was to evaluate and compare the radiosensitizing properties of gadolinium nanoparticles (NPs) with the gadolinium contrast agent (GdCA) Magnevist® and to better understand the mechanisms by which they act as radiation sensitizers. This was determined following either low energy synchrotron irradiation or high energy gamma irradiation of F98 rat glioma cells exposed to ultras-small gadolinium NPs (GdNPs, 3 nm) or GdCA. Clonogenic assays were used to quantify cell survival after irradiation in the presence of Gd using monochromatic X-rays with energies in the 25 keV-80 keV range from a synchrotron and 1.25 MeV gamma photons from a cobalt-60 source. Radiosensitization was demonstrated with both of these agents in combination with X-irradiation. At the same concentration (2.1 mg/mL), GdNPs showed a more important effect than GdCA. The maximum sensitization-enhancement ratio at 4 Gy (SER_{4Gy}) was observed at 65 keV irradiation energy, both for the nanoparticles and the contrast agent: $SER_{4Gy} = 2.47 \pm 0.30$ and 1.41 ± 0.15 , for GdNPs and GdCA, respectively. At high energy (1.25 MeV), radiosensitization was observed with GdNPs only: $SER_{4Gy} = 1.59 \pm 0.13$ and 1.02 ± 0.13 , for GdNPs and GdCA, respectively. The radiation dose enhancements were highly “energy dependent” for both agents, which allowed us to better understand the fundamental mechanisms that were involved. Photoactivation appeared to be the primary mechanism by which Gd contrast agents can function as radiosensitizers. Other mechanisms, such as alterations in the cell cycle and proliferation may explain the enhanced radiosensitizing properties of GdNPs.

Keywords: Gadolinium, nanoparticles, contrast agent, photoactivation, radiosensitization, X-rays

BACKGROUND

High grade gliomas are the most common primary malignant brain tumor in adults. They are almost invariably fatal with the current standard therapy consisting of surgery, radiotherapy and the concomitant administration of temozolomide (TMZ) followed by repetitive cycles of the latter treatment [1, 2]. Although the increase in overall median survival was only 2.5 months (14.6 vs 12.1 months), approximately 25% of patients were still alive at 2 years compared to less than 10% for those that did not received TMZ. The poor prognosis of patients with high grade gliomas highlights the necessity of evaluating new therapeutic approaches. Nanoparticles (NPs) are being evaluated as theranostics for radiation therapy. Hainfeld *et al.* [3] have shown that gold nanoparticles (AuNPs) could enhance the efficacy of radiation therapy for the treatment of the EMT-6 murine mammary carcinoma, and more recently a murine brain tumor model [4]. This therapeutic approach, initially proposed by Norman *et al.* [5] was based on the principle that the physical dose delivered locally to a tumor could be enhanced by the photon interactions that would occur within a tumor that had been loaded with high-Z atoms [6, 7]. The first studies were performed using molecular contrast agents (CA) and low energy X rays (<100 keV), where the photoelectric effect's cross-section was maximal compared to water. In the present study we have used gadolinium, which has been widely used clinically as a contrast agent (CA) but it also could be used as a photoactivator [8, 9]. When irradiated with X-rays, Gd generates electrons that have a kinetic energy equal to the difference between the incident photons' energy and the electron binding energies. K-edge photoelectrons (15 keV) created by photoionization of Gd atoms by 65 keV photons have a mean path length in water of ~ 8 μm , which is similar to the diameter of a cell. In this case, extracellular Gd atoms could have a direct effect on cell survival if a sufficient quantity of Gd atoms is localized in proximity or within the cell. Furthermore, following a K-edge photoelectric event, K-shell vacancies are created and subsequently filled with higher orbital electrons. The electronic re-organization of the Gd atoms yields a cascade of either fluorescence X-rays or Auger electrons that have very low energies, which are deposited very close to their site of production [10, 11].

If the high-Z atoms remain external to the cell nucleus, Auger electrons would not reach the nucleus but could damage other cellular targets such as the cell membrane and mitochondria.

Using high energies, such as those produced by a linear accelerator (LINAC), the photoelectric effect would no longer predominate and much lower dose enhancement factors (DEFs) would be expected. Monte Carlo simulations have been developed to evaluate the physical dose-enhancement induced by the presence of the high Z elements, based on their homogeneous distribution within a cell [7, 12, 13]. For example, Robar *et al.* [14] have reported on the DEFs simulated in a numeric head phantom for different Gd concentrations in the tumor as a function of the radiation energy. The calculated DEFs were 1.2 and 5.3 for a 2 MeV or 60 keV X-ray beam, respectively, with 30 mg/mL of Gd in the tumor [14]. The calculated and experimental dose-enhancement factors (DEF) were found to be in good agreement at a macroscopic scale in other studies [15, 16].

Although most studies refer to larger DEFs in the keV range, as predicted theoretically, radiosensitization at MeV photon energies also has been reported with NPs [17, 18]. Jain *et al.* [19, 20] have observed dose enhancement greater than MC simulations after irradiation of MDA-MB-231 breast cancer cells at MeV photon energies with 1.9 nm AuNPs. However, contradictory results also have been reported depending on the energy range considered [21-25]. Recently, Mowat *et al.* [26, 27] have utilized ultrasmall GdNPs as radiosensitizers for tumor cells. The NPs consisted of a core of gadolinium oxide surrounded by a shell of polysiloxane and were functionalized by diethylenetriaminepentaacetic acid (DTPA). These also have been used *in vivo* for the treatment of 9L gliosarcoma bearing rats in combination with X-ray microbeams ($E < 150$ keV) [28]. The median survival time was extended to 90 days compared to 47 days for irradiation alone. The underlying mechanisms by which radiosensitization increased in presence of the NPs following irradiation are still unclear. Monte Carlo simulations have shown that the assembly of heavy atoms within the NPs strongly modified the dose patterns at the nanoscale. Radiation doses were found to be higher within a few nanometers surrounding the NPs compared to those measured in water when using either high energy (MeV) X-rays or those in the photoelectric domain. However, simulations predicted that the

enhancement was much greater using kilovoltage energies compared to high energy X-rays [21, 23, 24, 29].

Since the physical DEF is strongly energy dependent [10, 15, 21, 30-34], monochromatic radiation produced by a synchrotron source provides a unique tool for evaluating the mechanisms by which radiosensitization occurs and can be used to differentiate between physical and biological contributors to dose enhancement. The aim of the present study was to evaluate the *in vitro* radiosensitizing effects produced by ultras-small GdNPs compared to those produced by GdCA, homogeneously distributed around the cells during irradiation and for different energies. In order to determine the relative importance of physical and biological contributions to the overall observed radiosensitizing effects on rat glioma F98 cells, clonogenic assays were performed using different incubation and irradiation conditions with either monochromatic X-rays from a synchrotron source (7 energies from 25 keV to 85 keV) or a cobalt-60 source (1.25 MeV).

METHODS

Gadolinium compounds

GdNPs (3 nm in diameter) were provided by Nano-H (Lyon, France). A detailed description of their synthesis and properties has been reported elsewhere [35]. Briefly summarized, they were composed of 8.5 ± 0.1 kDa particles containing 10 molecules of 1,4,7,10-tetraazacyclododecane-1,4,7,10-tetraacetic acid (DOTA), 7 Gd and 27 Si atoms per particle. The NPs were labeled with fluorescein isothiocyanate (FITC). The Gd contrast agent (GdCA) Magnevist[®] (14) chemical formula $C_{28}H_{54}GdN_5O_{20}$, molecular weight of 938 Da, was obtained from Bayer Schering Pharma, Berlin, Germany.

F98 cells

F98 glioma cells were purchased from the American Type Culture Collection, Manassas, VA (ATCC, # CRL-2397) and they have been described in detail by Barth and Kaur (36). These cells are known to have a highly invasive pattern of growth and being weakly immunogenic (36).

Determination of gadolinium nanoparticles uptake

Gd uptake was determined by means of ICP-MS using a Thermo X serie II, spectrometer (Thermo Electron, Bremen, Germany), which was equipped with an impact bead spray chamber and a standard nebulizer (1 mL/min). Three different treatment times were investigated, 30 min, 2h and 5h, following incubation with GdNPs at a concentration of 2.1 mg Gd/mL. For Gd determinations, the cells were washed twice in PBS, trypsinized (Trypsine EDTA 0.05% - Invitrogen), suspended in 1 mL of PBS, and then counted. Nitric acid was then added to the cell suspensions (final concentration 1%) and Gd concentrations were determined using an external calibration curve. Two stable Gd isotopes (^{155}Gd and ^{157}Gd) were measured and rhodium (^{103}Rh) was used as an internal standard. Determinations were carried out in triplicate.

Cell cycle distribution

The cell cycle distribution of F98 cells incubated with GdNPs (2.1 mg/mL, 5h) was determined from DNA histograms measured by flow cytometry. After incubation, the culture medium was decanted and the cells were trypsinized, washed twice with PBS and fixed with a 2% formalin solution. Cell membranes were permeabilized with 0.2% Triton X-100 in PBS. DNA was determined by fluorescent staining with DAPI (10 $\mu\text{g/mL}$) with a flow cytometer (LSR II, BD Bioscience, Franklin Lakes, USA). Cell cycle distribution was determined either immediately or 24 h after incubation with GdNPs and compared to untreated control cells. Cell cycle analysis was performed after doublet exclusion using FlowJo software (Tree Star, INC. Ashland, OR) and Watson DNA peak deconvolution.

Cell irradiations

Three treatment conditions were evaluated: 1) untreated control cells; 2) cells incubated for 5h with 2.1 mg/mL GdNPs; and 3) cells irradiated in the presence of 2.1 mg/mL GdCA (Magnevist®). Before irradiation, cells were trypsinized, washed and re-suspended in 200 μL of DMEM complete media (with or without Gd) and irradiated in Eppendorf tubes.

Low energy monoenergetic X-rays (from 25 to 80 keV) were produced from a synchrotron source at the European Synchrotron Radiation Facility (ESRF - biomedical ID17 beamline -

$\Delta E/E \approx 0.1\%$). The dosimetry was performed using an ionization chamber (PTW Semiflex ion chamber 31010 – 0.125 cm³). High energy irradiations were carried out using a cobalt-60 source, which emitted gamma photons with energies of 1.17 and 1.33 MeV (1.25 MeV mean energy). For radiosensitization versus photon energy, cells were irradiated at a single 4 Gy dose with beam energy 31.0, 40.0, 49.5, 51.0, 65.0, 80.0 keV and 1.25 MeV. For dose-response curves, samples were irradiated with 0, 2, 4 or 6 Gy and with a beam energy of 51 keV (just above the Gd K-edge).

Clonogenic assays

Clonogenic assays were used for determining the sensitizing enhancement produced by Gd in combination with X-irradiation. Following treatment, the cells were counted and diluted in the appropriate volume of DMEM. Three different cells concentrations were seeded in triplicate into Petri dishes (100 mm diameter) containing 8 mL of complete DMEM. The petri dishes were incubated at 37°C in an atmosphere containing 95% air and 5% CO₂ for 11 days. All experiments were repeated three times. Following staining with crystal violet, colonies of greater than 50 cells were enumerated. The surviving fractions (SF) were determined as the ratio of the number of colonies counted divided by the number of cells plated, normalized to un-irradiated controls.

Cell survival and sensitization-enhancement ratio at 51 keV

Radiation dose response curves obtained at 51 keV were fitted by the linear quadratic (LQ) model: $S = e^{-(\alpha D + \beta D^2)}$ with, D (Gy) the radiation dose, S the normalized survival fraction and two parameters, α (Gy⁻¹) and β (Gy⁻²). The α parameter characterizes the first part of the slope of the cell survival curve and the effectiveness at low doses, while β represents the contribution from cumulative damages, presumably due to the interaction of two or more lesions. The α/β ratio represents the dose at which the linear and quadratic terms contribute equally to the total effect. The sensitizing Enhancement Ratio (SER) was calculated as the ratio of the Survival fraction for control cells (computed with the corresponding α and β parameters) to that of cells irradiated in combination with Gd.

Sensitization-enhancement ratio versus energy

The sensitizing Enhancement Ratio *versus* energy (SER_{4Gy}) was defined as the ratio of the SF for control cells (4 Gy irradiation alone) to that of cells irradiated with 4 Gy with Gd.

Statistical analysis

All experiments were performed 3 times with triplicate samples in each study and the final data represented the means from the three independent experiments. The statistical errors corresponded to their standard deviation (SD) and the error bars on graphs indicated 1 SD. Statistical differences between the experimental results were evaluated using Student's two-tailed t-test, which was the most suitable method for the analysis of small samples ($n < 30$). Differences were considered significant at the level of $p \leq 0.05$.

Computed Macroscopic Dose-Enhancement Factor (DEF)

Monte Carlo simulations (MCNPX version v27e) were used to estimate the macroscopic physical dose enhancement produced by Gd during irradiation. The input geometry was defined by a cube (1 cm^3 , imbedded in air) containing either water or a solution of Gd mixed homogeneously in water at a concentration of 2.1 mg Gd/mL. The dose enhancement factor (DEF) was defined as the ratio between the doses deposited in the cube containing Gd to that deposited in a cube only containing water. DEFs were calculated for the same energies as those used for cell irradiations between 25 keV to 1.25 MeV and using 10^8 incident photons per irradiation to obtain uncertainties $< 5 \%$. A square source ($2 \times 2 \text{ cm}$) was centered on the cube and placed at a distance of 4.5 cm in front of it.

Computed Sensitization-enhancement Ratio

The theoretical sensitization-enhancement ratio (SER) is calculated, assuming that radio-sensitization in presence of Gd is uniquely induced by physical effects. The normalized survival fraction in presence of Gd (SF_{Gd}) is calculated using the parameters α and β (obtained from the $SF_{control}$) and the computed dose-enhancement factor (DEF), as follows:

$$SER = SF_{control}/SF_{Gd}$$

$$SF_{control} = \exp(-\alpha D - \beta D^2)$$

$$SF_{Gd} = \exp(-\alpha D \times DEF - \beta (D \times DEF)^2)$$

$$SER = SF_{control}/SF_{Gd}$$

$$SER = \exp(\alpha D \times (DEF - 1) + \beta D^2 (DEF^2 - 1))$$

With:

- SF_{Gd} and $SF_{control}$, the normalized survival fractions measured experimentally with and without Gd, respectively.
- α and β are the control cells radiosensitivity parameters (in absence of radio-sensitizer) extracted from the $SF_{control}$ curve using the LQ model.
- The DEF is calculated using Monte Carlo simulations, as previously described.

RESULTS

Radiosensitization versus radiation dose, measured above the Gadolinium K-edge.

In order to assess the radiosensitization potential of GdNPs, F98 glioma cells were incubated for 5 h with 2.1 mg/mL of GdNPs, then irradiated with a monochromatic photon beam at 51 keV. For comparison, F98 cells were also irradiated with 0, 2.1, 5.0 or 10.0 mg/mL of GdCA in the culture medium. At 0 Gy, SF of F98 cells incubated with GdNPs was 0.96 ± 0.11 . The normalized survival values with the contrast agent were 1.00 ± 0.15 , 1.01 ± 0.15 , 1.08 ± 0.17 and 1.07 ± 0.14 , for the 4 increasing GdCA concentrations respectively, indicating that both agents were non-toxic in these experimental conditions. The survival curves *versus* X-ray dose are shown in Figure 1. The cell radiosensitivity parameters α and β are shown in Figure 2 for all control and treated cells conditions. Gadolinium induced cells radiosensitization in all cases. Both GdNPs and GdCA induced a large increase of the linear parameter α , and a decrease of β . For GdCA, the increase of α depends on the Gd concentration (Figure 2). The sensitization-enhancement ratios in presence of Gd compounds *versus* the radiation dose are shown in Figure 3. The sensitization-enhancement ratios reach a plateau after 5 Gy, when cells were irradiated in presence of GdNPs. On the contrary, in presence of GdCA, the SERs increase, both with Gd concentration and X-ray dose.

Radiosensitization versus photon energy measured at 4 Gy

Figure 4 summarizes the SER_{4Gy} measured for GdNPs and GdCA in comparison with the theoretical SER_{4Gy} . The experimental sensitization factors for GdCA, were in good agreement with theoretical SER_{4Gy} at all energies. As expected, the greatest enhancement was obtained at 65 keV and no radiosensitization was observed when irradiation was performed at high energy (1.25 MeV) (Figure 4). Cells irradiated in presence of GdNPs had significantly higher SER_{4Gy} values compared to GdCA at all energies. As for GdCA, the highest sensitization enhancements were obtained when the cells were irradiated at 65 keV. A significant increase of the SER_{4Gy} was observed above and below the Gd K-edge (50.25 keV). GdNPs also led to a radiosensitizing effect for high-energy irradiations.

GdNPs quantification

The kinetics for the uptake of GdNPs by F98 cells was determined by means of ICP-MS. The amount of Gd increased and reached a plateau of up to 0.60 ± 0.06 pg Gd/cell after 5 h of incubation at 37°C with GdNPs at a concentration of 2.1 mg/mL (Figure 5).

Cell cycle distribution

Figure 6 depicts the proportions of F98 cells in different phases of the cell cycle for control cells and those incubated for 5 h with 2.1 mg/mL GdNPs. Immediately after incubation, no significant differences were observed between the two conditions ($p > 0.5$), for all phases. Twenty-four hours after termination of the incubation with GdNPs, a significant cellular accumulation was measured in G2/M phase ($p < 0.05$).

Discussion

The important finding in the present study was that differences were observed between the radiosensitizing effects produced by Gd in the form of ultras-small NPs and those produced by GdCA. Radiosensitization was strongly energy dependent for both chemical forms of Gd. Irradiation of F98 cells in the presence of GdNPs led to a significantly greater enhancement of radiosensitization than that produced by GdCA for the same concentration. The experimental SER_{4Gy} was energy dependent and reached a maximum at 65 keV (energy of theoretical

maximum SER) of 2.47 ± 0.30 , compared to 1.41 ± 0.15 for GdCA. In addition, GdNPs led to a significant increase in the SER_{4Gy} for irradiations carried out above the Gd K-edge compared to that below the K-edge. This indicated that the photoelectric effect played a major role in the observed radiosensitivity enhancement. However, the SER_{4Gy} also was found to be significantly greater than 1 for high-energy X-irradiation in presence of GdNPs, although theoretically, only minimal dose enhancement was expected at this energy (Figure 4). There are two possible hypothesis to explain the observed radiosensitization effect with GdNPs. Firstly, taking into account the structure of the NPs, the secondary electrons produced in the NPs deposit their energy in the immediate vicinity of the NPs and create very hot points of doses which can impair the cell structures, as determined by MC simulations (Delorme R. unpublished data). Secondly, biological mechanisms that make cells more sensitive to radiation also could be involved in the radiosensitization observed in the presence of GdNPs and this would explain the large SER values observed with high energy X-rays. Additional experiments have been performed to measure perturbations in cellular metabolism following exposure to GdNPs. Both cell cycle regulation and cell proliferation were affected by incubation with GdNPs. Proliferation temporarily was slowed down for up to 4 days after incubation (data not shown) and an accumulation of cells in G2/M phase was observed at 24h after incubation (Figure 5). Other investigators have reported similar results that were cell line and NP type dependent. Coulter et al. [19] reported that MDA-MB-231 cells exhibited proliferation arrest and a sub-G1 accumulation after an exposure to $12 \mu M$ of 1.9 nm AuNPs, whereas L132 cells were not affected after a similar exposure.

A good agreement was obtained between the experimental data and the calculated DEFs *versus* the photon energy (both low and high energies), for the contrast agent GdCA. This suggests that the physical dose enhancement induced by photoelectric effects on Gd atoms is the predominant mechanism that produced cell death. As predicted theoretically by MC simulations (Delorme *et al.* unpublished data) [21], no sensitization enhancement was observed following irradiation with 1.25 MeV photons from a cobalt 60 source. The

radiosensitization effect was directly proportional to the concentration of the high Z atoms contained in the medium. Regarding the survival curves, the linear α component increased linearly ($R^2 > 0.95$) with GdCA concentration (Figure 2), which indicates that the main effect is an increase in the number of directly lethal events due to the presence of Gd. The β value was not significantly changed, indicating an intact repair of sub lethal damages [36].

In presence of nanoparticles, a marked increase of the linear α component was obtained (factor 150 relative to controls) and the quadratic term β becomes negligible (Figure 2). Similar results were obtained with other cells lines and GdNPs [37]. This might be explained by cell cycle perturbations that occur in presence of GdNPs. Further investigations are warranted to support this hypothesis.

Differences of the sensitization-enhancement ratio between GdNPs and GdCA were also observed *versus* the X-ray dose as shown in Figure 3. For cells irradiated in presence of nanoparticles, a saturation is observed above 4 Gy (SER ~ 2 at 51 keV). On the contrary with Gd contrast agent, the sensitization-enhancement factors continue to increase, both with the radiation dose and the Gd concentration (SER ~ 4 at 6 Gy in presence of 10 mg/mL of GdCA). These results suggest that it could be favorable to choose radiation doses ~ 4 Gy when using GdNPs, such doses are comparable to classical radiotherapy treatment fractionation.

In the present study we have demonstrated that F98 glioma cells took up ultras-small GdNPs without leading to a significant decrease in survival. Uptake of GdNPs was time dependent and reached a plateau after a 5h of incubation with 2.1 mg Gd/mL. GdNPs increased the F98 cells' radiosensitivity primarily for keV photon energies with a larger effect than that observed with the same concentration of GdCA. Based on our data, we have concluded that radiosensitization of GdNPs could be attributed to two mechanisms. First, the photoelectric effect enhancement in the keV energy range, and second to biological interactions of GdNPs with the cells, resulting in proliferation arrest and the accumulation of cells at the G2/M interface of the cell cycle. In summary, our data provide strong support for the radiosensitizing effect of

ultrasmall GdNPs over a broad energy range, even at high energies such as those used in conventional radiotherapy. Preliminary experiments have shown that the GdNPs are non-toxic when directly injected into the rats brains (110 μg Gd in 5 μL injected over 10 min, unpublished data). Further *in vivo* pre-clinical studies on their circulation time and tumor uptake are warranted to further define the potential clinical benefit of ultrasmall GdNPs as radiation sensitizers.

Figure Legends

Figure 1: Radiosensitizing effects of GdNPs and GdCA. All irradiations were performed with 51 keV monochromatic X-rays.

- A. F98 cells survival curves for control cells (○) and for cells incubated for 5h with 2.1 mg/mL of GdNPs (Δ).
- B. F98 survival curves for control cells (●) and cells irradiated in presence of 2.1 mg/mL (▲), 5.0 mg/mL (■) and 10.0 mg/mL (▼) of GdCA.

Figure 2: α (Gy^{-1}) and β (Gy^{-2}) parameters derived from the linear quadratic fits of survival curves for F98 cells treated with 2.1 mg/mL of GdNPs (●) and (▲), for α and β , respectively or 0, 2.1, 5.0 and 10.0 mg/mL of GdCA (○) and (Δ), for α and β , respectively. The irradiations were performed with 51 keV monochromatic X-rays. For GdCA, the plots of α and β versus Gd concentration were both adjusted with a linear function (dotted lines, $R^2 > 0.95$).

Figure 3: Sensitization-enhancement ratios versus X-ray dose. All irradiations were performed with 51 keV monochromatic X-rays. F98 cells incubated for 5h with 2.1 mg/mL of GdNPs (Δ). F98 cells irradiated in presence of 2.1 mg/mL (▲), 5.0 mg/mL (■) and 10.0 mg/mL (◆) of GdCA.

Figure 4: $\text{SER}_{4\text{Gy}}$ of F98 cells irradiated at various X-ray energies with Gadolinium (2.1 mg/mL) Theoretical $\text{SER}_{4\text{Gy}}$ (✕) calculated for a homogeneous distribution of Gd, compared to $\text{SER}_{4\text{Gy}}$ of F98 cells irradiated in presence of GdCA (■) or in presence of GdNPs (Δ).

Figure 5 : Uptake of GdNPs by F98 cells as a function of the incubation time (t) assessed by ICP-MS. Data were adjusted by $\alpha \cdot t^\beta$, with $\alpha=0.37\pm 0.03$, $\beta=0.34\pm 0.05$ and $\chi^2=1.1$.

Figure 6: Distribution of F98 cells in the different phases of the cell cycle (G1, S and G2/M) for control cells (dark grey) and cells incubated for 5h at 37°C with 2.1 mg/mL GdNPs (light grey).
a) Cell cycle distribution immediately after 5h incubation. b) Cell cycle distribution at 24 h after the end of the incubation period.

Figure 1:

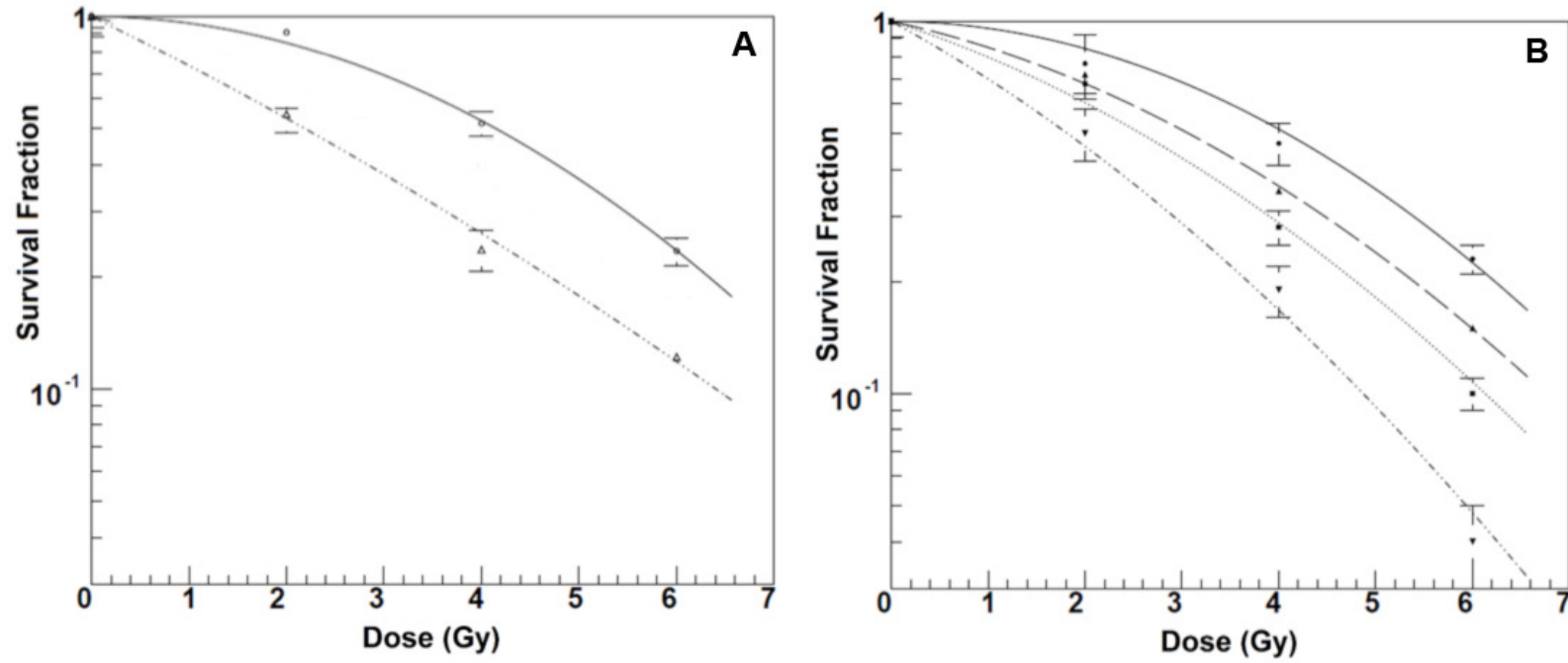


Figure 2 :

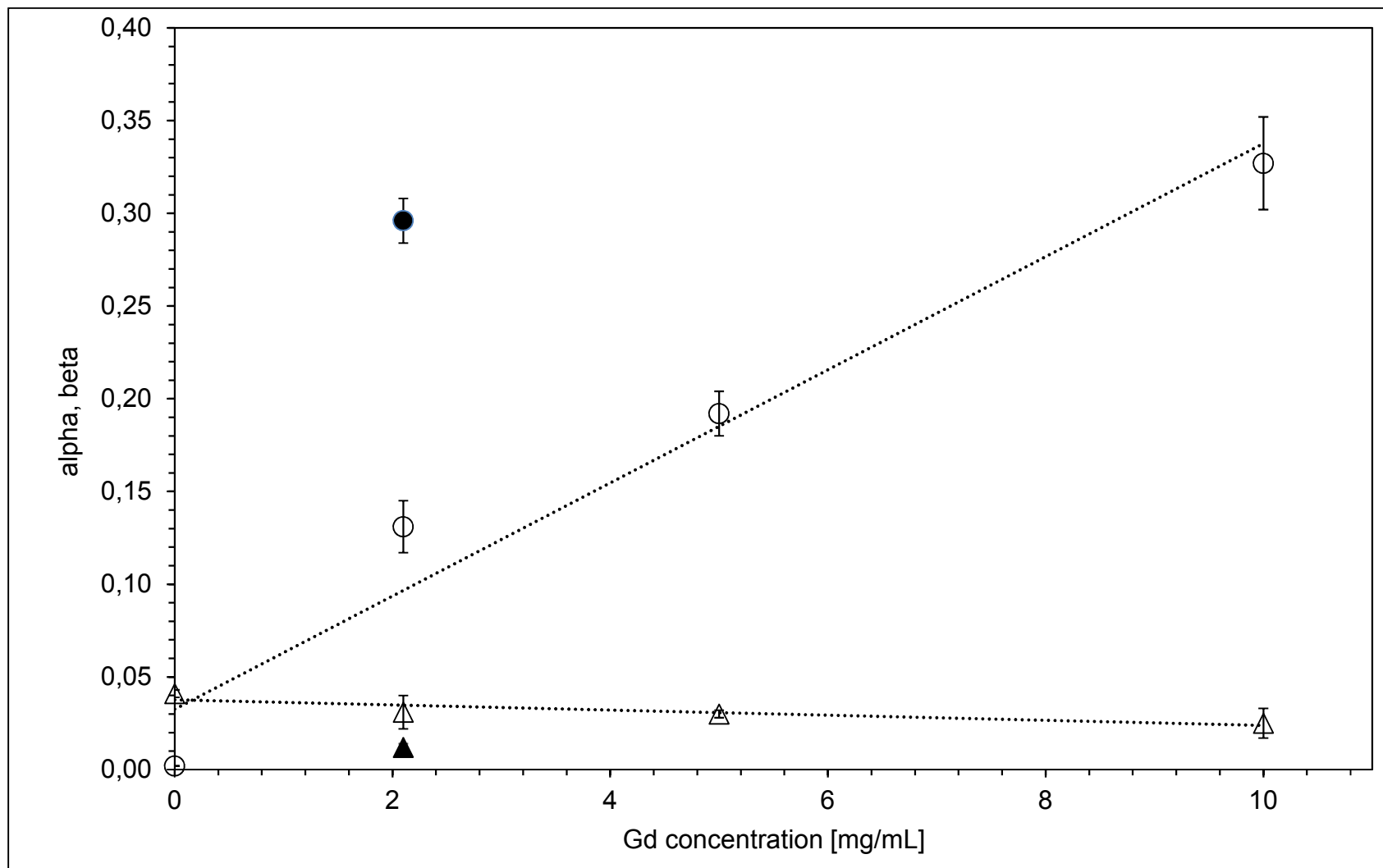


Figure 3 :

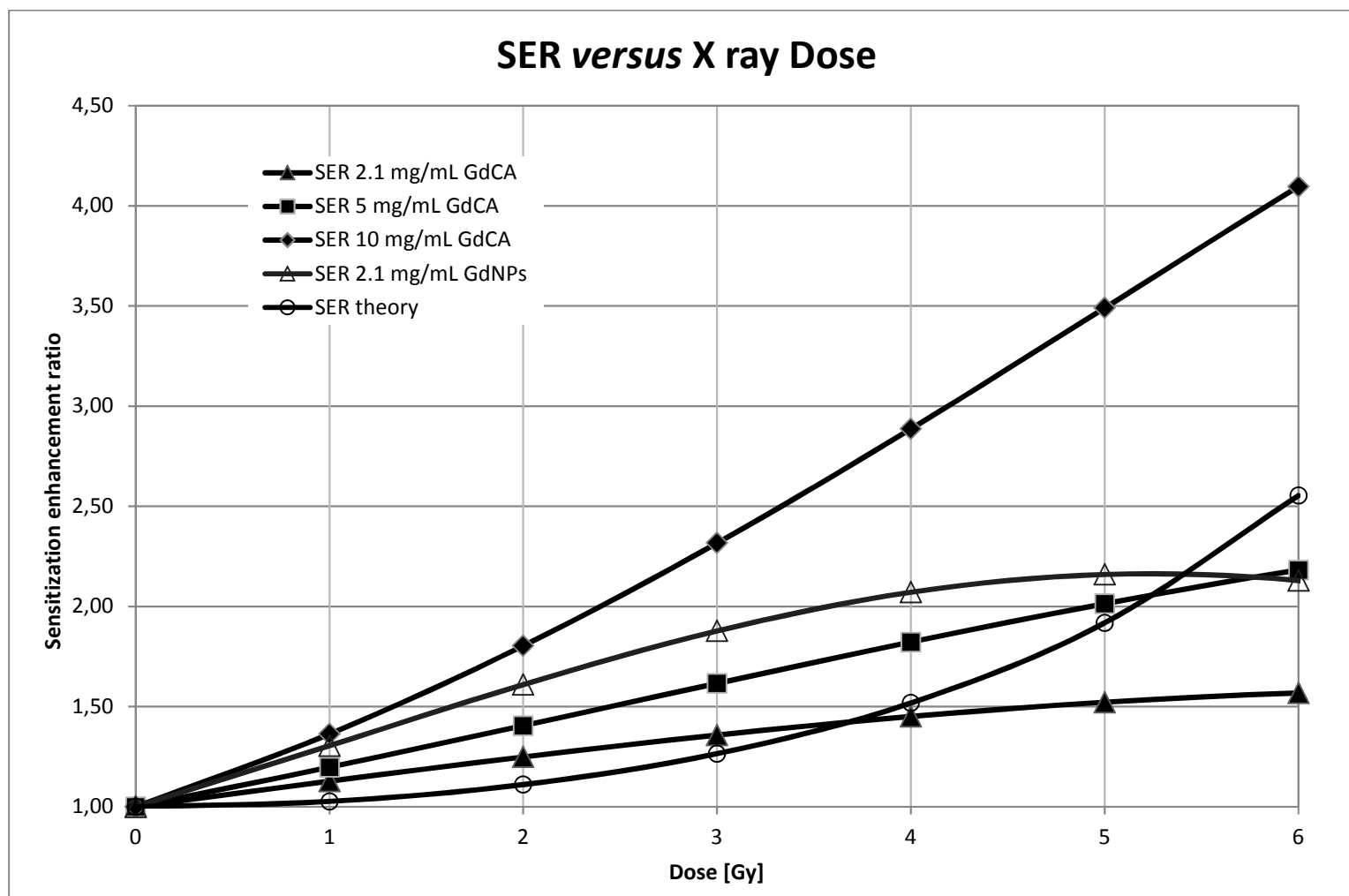


Figure 4:

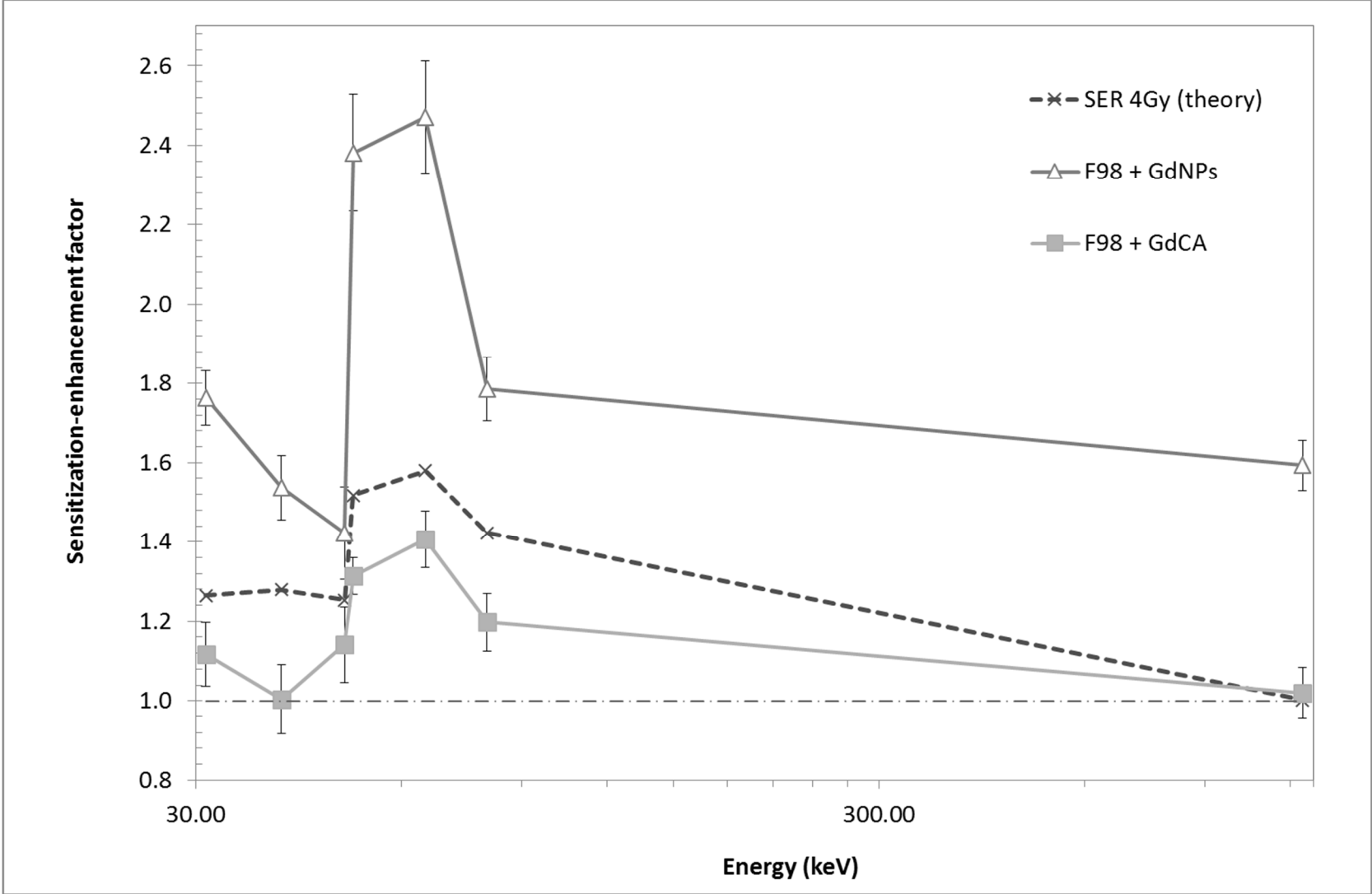


Figure 5:

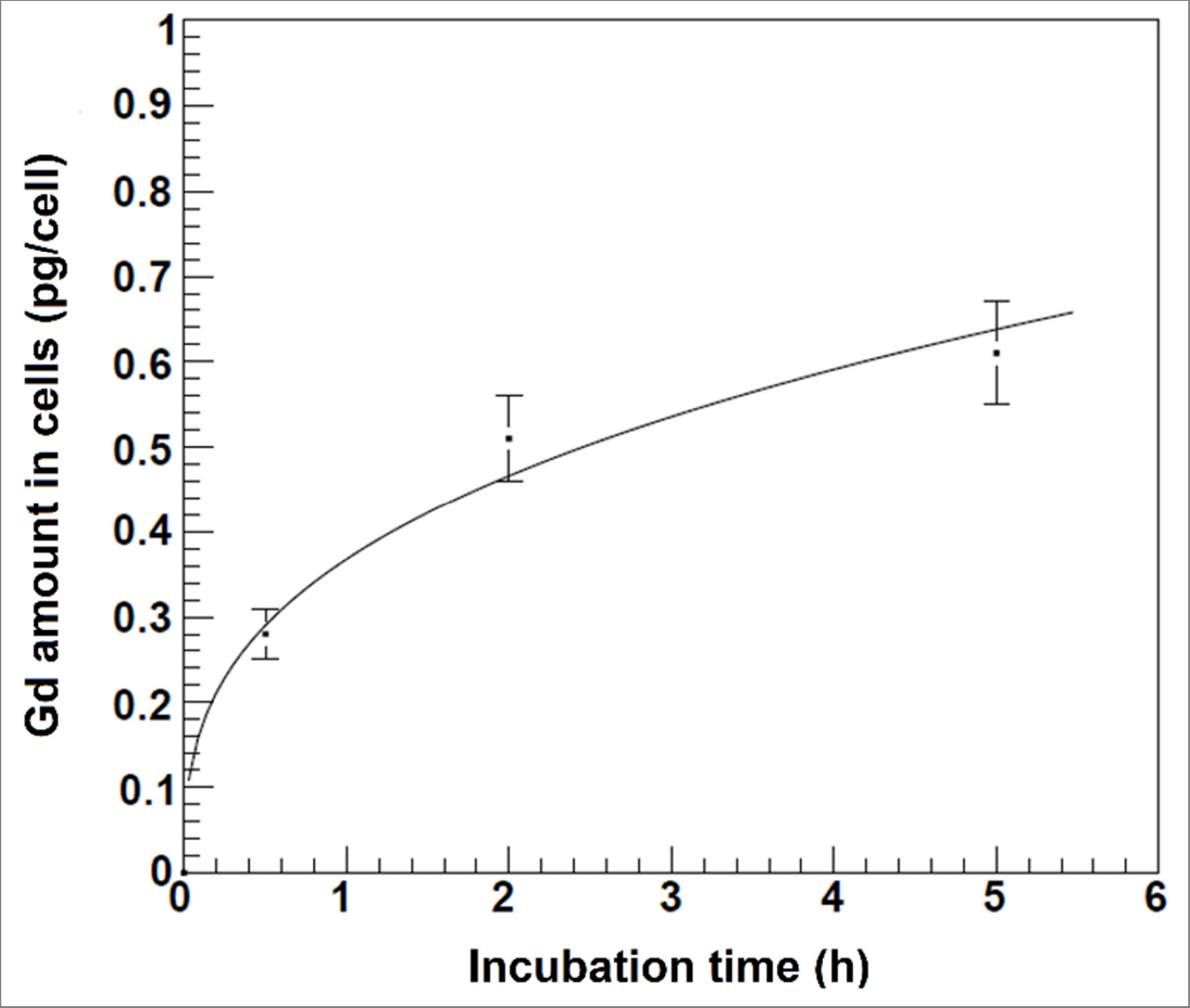
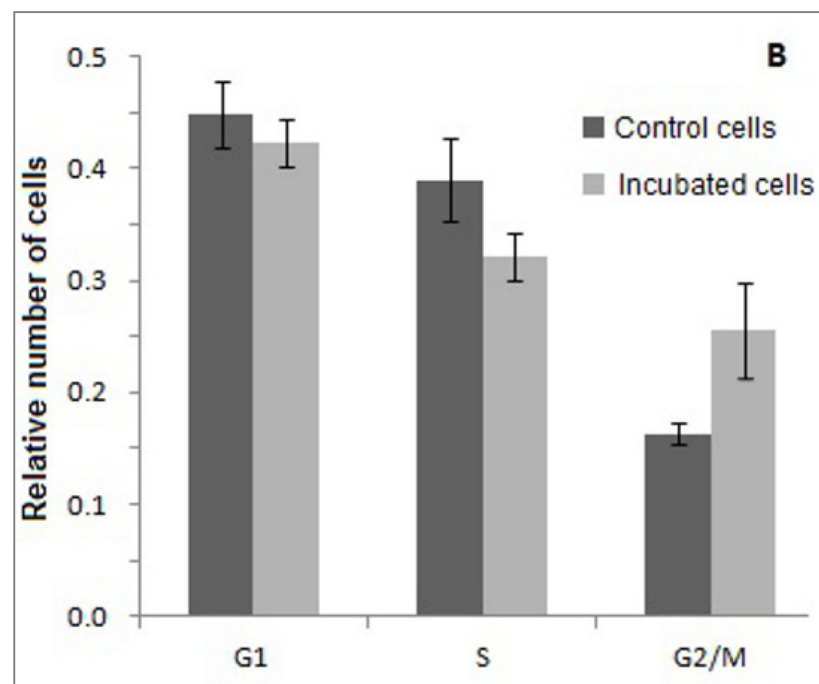
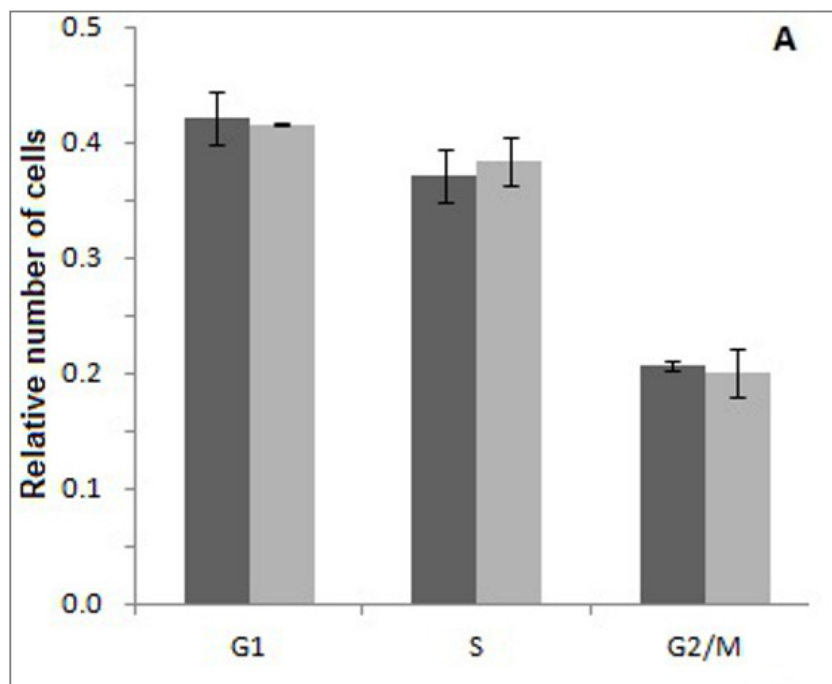


Figure 6:



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